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MICROSCOPIC NMR IMAGING

A thesis presented in partial fulfilment of the requirements for the degree of Doctor of Philosophy in Physics at Massey University

by

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ABSTRACT

A commercial 60MHz nuclear magnetic resonance spectrometer has been modified to perform non-invasive, high resolution, two dimensional proton density imaging on samples smaller than 10mm.

Orthogonal magnetic field gradients are applied during the experiment to impart a spatial tag to the nuclear spins. The resultant nuclear signal detected by the spectrometer corresponds to a sampling of Fourier space. The exact trajectory in this space depends on the magnitude and timing of the applied gradients. The technique used in this work samples k space in a radial fashion and is termed filtered back projection. Image reconstruction is implemented on a 16 bit personal computer using a two dimensional fast Fourier transform algorithm.

Due to the small volume elements employed the available signal to noise ratio limits the resolution attainable. It is therefore important that the S/N be maximized within the system. To this end careful attention has been paid to the transfer of the nuclear signal from sample to spectrometer. Signal averaging is also used to improve the S/N although this does result in long imaging times (typically 30 to 60 minutes). At present a resolution of about 30 µm is achievable for a slice thickness of 1.5mm and a S/N of 40. At the time of initial publication in June 1986, this corresponded to a voxel resolution an order of magnitude better than that obtained by other workers in this field.

The orthogonal field gradients used are capable of generating gradients of up to $2Tm^{-1}$. This provides the possibility of measuring self diffusion coefficients in an intact sample, using the pulsed field gradient spin echo technique – something which would be difficult to achieve with a large scale imaging system. This thesis reports the first measurements of localised self-diffusion coefficients using a combination of the PFGSE technique and NMR imaging.

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SYMBOL TABLE

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|----------------|--|--------------|-----------|-----------|------|
| Α | Cross sectional area of rf coil | | | | 41 |
| B_0 | Main magnetic field, directed along the z axis | 5. | | | 3 |
| B ₁ | Magnetic field due to applied rf. | | | | 6 |
| C | Spatial resolution contrast ratio. | | | | 54 |
| dV | Volume element | | | | 16 |
| F | Fourier transform operator | | | | 19 |
| F | Noise factor of spectrometer | | | | 41 |
| F(n) | Filter function | | | | 49 |
| fr | Frequency corresponding to the edge or a cyl | inder of ra | dius r. | | 63 |
| G | Magnetic gradient vector | | | | 16 |
| ħ | Planck's constant/ 2π | | | | 3 |
| 1 | Angular momentum vector | | | | 3 |
| 1 | Spin quantum number | | | | 3 |
| 1 | Coil current | | | | 40 |
| Im[] | Imaginary part of complex term in brackets. | | | | 49 |
| j | (-1)1/2 | | | | 16 |
| k | Reciprocal space position vector. | | | | 16 |
| k _B | Boltzmann's constant. | | | | 38 |
| L | Length of conductor used in rf coil. | | | | 42 |
| L | Inductance of rf coil | | | | 41 |
| Q | Length of rf coil | * * * | | | 38 |
| М | Magnetization vector | | | | 6 |
| m | Representation of r in the computer. | | | | 45 |
| m | Spin magnetic quantum number | | | | 6 |
| m_r | Number of data points representing the radius | s of a cylir | nder. | | 47 |
| n | Representation of k in the computer. | | | | 45 |
| Up. | Number of points characterising the decay of | f the filter | function. | | 50 |
| N | Number of data points in fid | | | | 33 |
| Nacc | Number of time domain accumulations. | | | | 33 |
| Nn | Number of hydrogen nuclei per unit volume. | | | | 6 |
| Nk | Noise level in k space. | | | | 49 |
| ND | Number of projection used in FBP. | | | | 37 |
| N _r | Naise level in image asses | | | | 49 |
| • | Number of turns on soil | • • • | | • • • | 38 |
| Nt | | | | • • • | |
| P | Principle part | | | | 67 |

[Symbol table]

| P <u>+</u> | Probability that the nuclear spir | n will be align | red (-) with | or oppose | $d (+) to B_0$. | | 38 |
|------------------|-----------------------------------|-----------------|--------------|-----------|------------------|-------|-----|
| P | Wire circumference. | | | | | | 42 |
| P ₂ | $= T_2 \Delta f$ | | | | | | 54 |
| Q | Quality factor of rf coil. | | | | | | 41 |
| Re[] | Real part of complex term in br | ackets. | | | | | 25 |
| R | Rf coil radius | | | | | | 38 |
| r | Image space position vector. | | | | | | 16 |
| r_c | Rf coil resistance | | | | | | 41 |
| r | Rf coil wire radius | | | | | | 38 |
| S(FBP) | Smoothing function used in FBP | | | | | | 71 |
| S(FZ) | Smoothing function used in FZ. | | | | | | 52 |
| Sk | Spatial frequency domain data. | | | | | | 45 |
| Sr | Image domain data | | | | | | 45 |
| Т | Total sampling time. | | | | | | 45 |
| T ₁ | Spin-lattice relaxation time. | | | | | | 10 |
| T ₂ | Spin-spin relaxation time. | | | | | | 10 |
| T ₂ * | Transverse relaxation time. | | | | | | 12 |
| Tc | Coil temperature in Kelvin. | | | | | | 41 |
| Tr | Experiment repetition time. | | | | | | 76 |
| Ts | Sample temperature in Kelvin. | | | | | | 38 |
| V _C | Volume of coil | | | | | | 42 |
| V _S | Volume of sample | | | | | | 38 |
| | | | • • • | | • • • • | | 99 |
| V _C | | | • • • | • • • | • • • | | |
| Vm | Modulation level | • • • | • • • | | | | 99 |
| | | | | | | | |
| 8 | Gyromagnetic ratio. | | *** | | | | 3 |
| Δſ | Frequency domain bandwidth of | spectromete | r. | | | | 41 |
| Δy | Slice thickness. | | | | | | 46 |
| Δz | Spatial resolution in the final i | mage. | | | | | 38 |
| Δω | Offset from resonance. | | | | • • • | | 146 |
| 8 | Skin depth | | • • • | | • • • | | 42 |
| θ | Tip angle | | | | | | 9 |
| Д | Magnetic moment vector. | | | | | | 3 |
| μ_0 | Permeability of free space. | | | • • • | | • • • | 40 |
| μr | Relative permeability. | | | | | | 42 |
| ξ | Induced EMF amplitude. | | | | | | 10 |
| P | Proton density function. | | | | | | 16 |
| ρ | Coil wire resistivity. | | | | | | 42 |

| [Symbol table] | 1.11.4 |
|----------------|--------|
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| | |

| Q | Coil proximity factor | | | 42 |
|------------|---|------|------|----|
| τ | Torque | | | 3 |
| τ | Short time interval | | | 12 |
| τ_{C} | Molecular correlation time | | | 10 |
| φ | Projection angle | | | 35 |
| Ψ | Filtered profile | | | 36 |
| ω_0 | Larmor precession frequency due to B_0 . | | | 5 |
| ω_1 | Larmor precession frequency due to B ₁ . | | | 8 |